

# Contributions of Lattice Computing to Medical Image Processing

Thesis dissertation

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# Motivation

This Thesis proceeds along two main lines:

- The exploration of new computational solutions based on the novel paradigm of Lattice Computing.
  - Lattice computing is the class of algorithms that either apply lattice operators  $\inf$  and  $\sup$ , involve the use of Lattice Theory results and operators lattice theory.
- The application to medical image data in order to obtain new image processing methods, and computer aided diagnosis systems based on image features that can be used as image biomarkers

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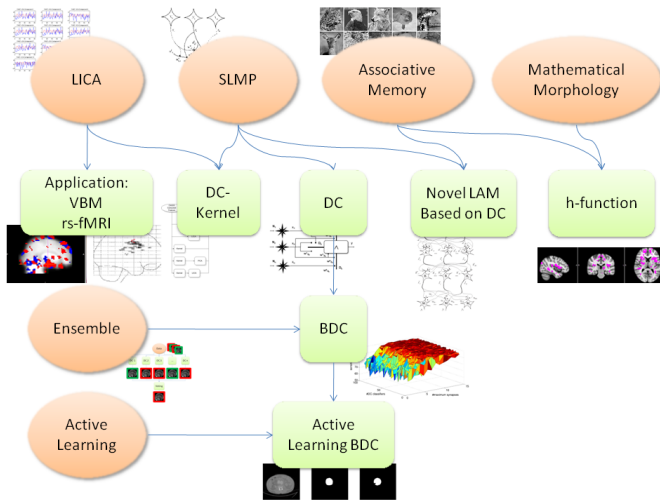
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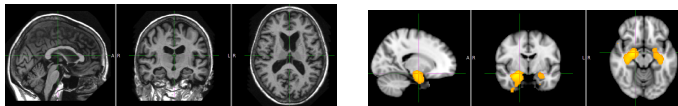


# Contents of the Thesis

- Results of **Dendritic Computing** approaches
  - Single Layer Morphological Perceptron (SLMP) improvement by introducing **shrinking hyperboxes**, and **Kernel LICA** preprocessing
  - **Ensembles of SLMP Dendritic Classifiers**
  - **Active learning**
  - A novel **Auto-Associative Memory**
- Results on the application of **LICA** on three case studies:
  - Voxel Based Morphometry on anatomical MRI
  - Segmentation of fMRI data, i.e. synthetic benchmark data
  - Connectivity in resting state fMRI
- **Application of Multivariate Mathematical Morphology** to resting state fMRI

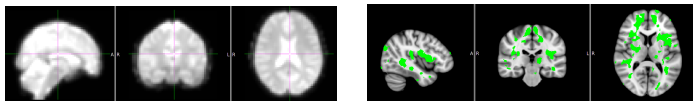


# Medical Image Processing



## Alzheimer's Disease

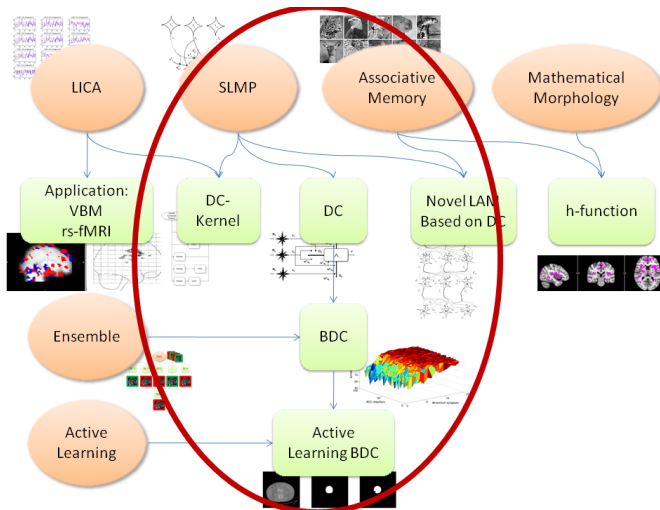
- Is a neurodegenerative disorder
- Features extracted from anatomical MRI brain volumes
- Is valuable as a benchmark dataset



## fMRI data

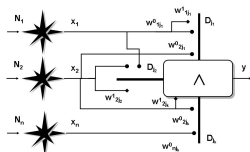
- Exploratory studies of LICA on synthetic benchmark fMRI data
- Connectivity studies on resting state fMRI data of Schizophrenia
  - LICA
  - Multivariate Mathematical Morphology

# Dendritic computing



# Dendritic computing

**Dendritic** Computing is based on the concept that dendrites are the basic information processing units of cortical neurons.



**Perfect** training accuracy: SLMP Dendritic Classifier has been proved to achieve perfect approximation of any data distribution.

**However**, they generalize badly when tested on conventional k-fold cross-validation schemes.

# Dendritic computing

In order to improve generalization of SLMP we have followed various paths:

- Application of hyperbox reduction factor, which relaxes perfect approximation to obtain some improvement in the testing phase
- Performing appropriate combination with data transformations, specifically with the LICA approach and a kernel transformation of the data
- Collection of weak Dendritic Classifiers into ensemble by majority voting, which we call Bootstrapped Dendritic Computing

# Dendritic computing

- Multi-layer Dendritic Computing allows to build robust Associative Memories
- Tested on a collection of heavily corrupted images

# Lattice matrix products

- Given matrices  $A$  and  $B$
- The matrix max-product operator denoted  $\boxtimes$  is defined as

$$C = A \boxtimes B = [c_{ij}] \Leftrightarrow c_{ij} = \bigvee_{k=1..n} \{a_{ik} + b_{kj}\},$$

- and the dual min-product matrix operator  $\boxdot$  is defined as

$$C = A \boxdot B = [c_{ij}] \Leftrightarrow c_{ij} = \bigwedge_{k=1..n} \{a_{ik} + b_{kj}\}.$$

# Lattice Associative Memory

- Input/output pairs of patterns

$$(X, Y) = \left\{ \left( \mathbf{x}^\xi, \mathbf{y}^\xi \right) ; \xi = 1, \dots, k \right\}$$

- A linear heteroassociative neural network

$$W = \sum_{\xi} \mathbf{y}^\xi \cdot \left( \mathbf{x}^\xi \right)'$$

- Erosive and dilative LAMs, respectively, are constructed as

$$W_{XY} = \bigwedge_{\xi=1}^k \left[ \mathbf{y}^\xi \times \left( -\mathbf{x}^\xi \right)' \right] \text{ and } M_{XY} = \bigvee_{\xi=1}^k \left[ \mathbf{y}^\xi \times \left( -\mathbf{x}^\xi \right)' \right],$$

where  $\times$  is any of the  $\boxtimes$  or  $\boxdot$  operators.

# Lattice Auto-Associative Memory

- When  $X = Y$  then  $W_{XX}$  and  $M_{XX}$  are called Lattice Auto-Associative Memories (LAAMs)
- LAAM have perfect recall for an unlimited number of stored patterns

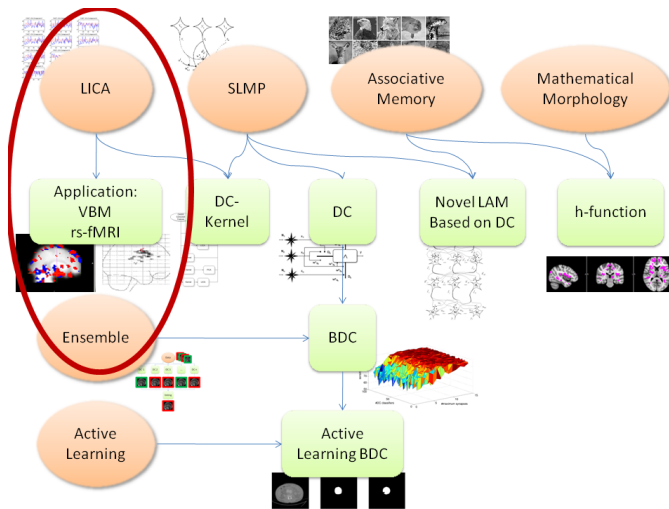
$$W_{XX} \boxtimes X = X = M_{XX} \boxtimes X$$

and

- Convergence in one step for any input pattern
  - if  $W_{XX} \boxtimes \mathbf{z} = \mathbf{v}$  then  $W_{XX} \boxtimes \mathbf{v} = \mathbf{v}$
  - if  $M_{XX} \boxtimes \mathbf{z} = \mathbf{u}$  then  $M_{XX} \boxtimes \mathbf{u} = \mathbf{u}$



# Lattice Independent Component Analysis



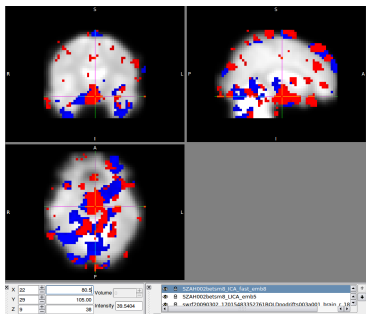
# Lattice Independent Component Analysis

**LICA** assumes that the data is generated as a convex combination of a set of endmembers which are the vertices of a convex polytope covering the input data.

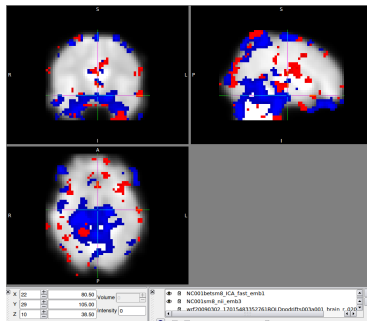
**This** assumption is similar to the linear mixture assumed by the ICA approach, however LICA does not impose any probabilistic assumption on the data.

**Applications:** analysis of fMRI data (synthetic datasets), Voxel Based Morphometry of structural MRI, and detecting functional connectivity in resting state fMRI.

# Lattice Independent Component Analysis



Patient

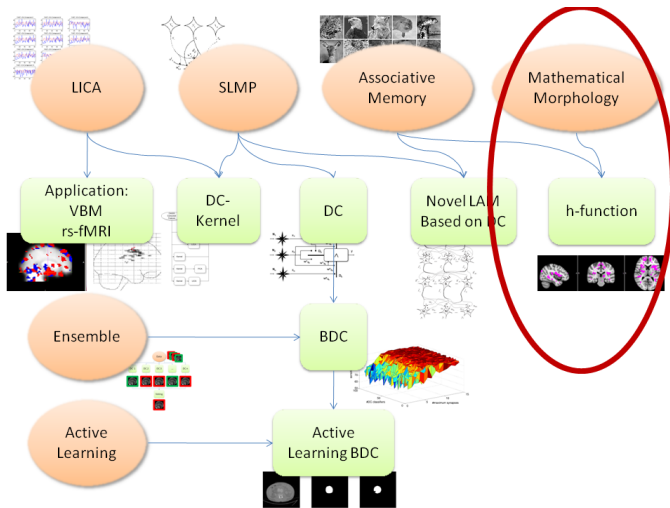


Control

Red corresponds to ICA detection, Blue to LICA detection.

Brain networks detected on Schizophrenia rs-fMRI by ICA and LICA approaches.

# Multivariate Mathematical Morphology (MMM)



# Multivariate Mathematical Morphology (MMM)

**Extension** of Mathematical Morphology from gray scale images to high dimensional vector images, i.e. functional Magnetic Resonance Images.

**Fundamental** issue in MMM is the definition of ordering over the multivariate data space ensuring morphological operators.

**Technique** consists in using the outputs of two-class classifiers trained on the data to build meaningful reduced orderings.

**Classes** are defined as foreground and background classes corresponding to target and background features of the data.

# Multivariate Mathematical Morphology

**LAAM.** We have introduced several approaches to define reduced supervised orderings based on the recall error of the LAAM.

**Application** - identify functional networks in resting state fMRI data looking for biomarkers of cognitive or neurodegenerative diseases.

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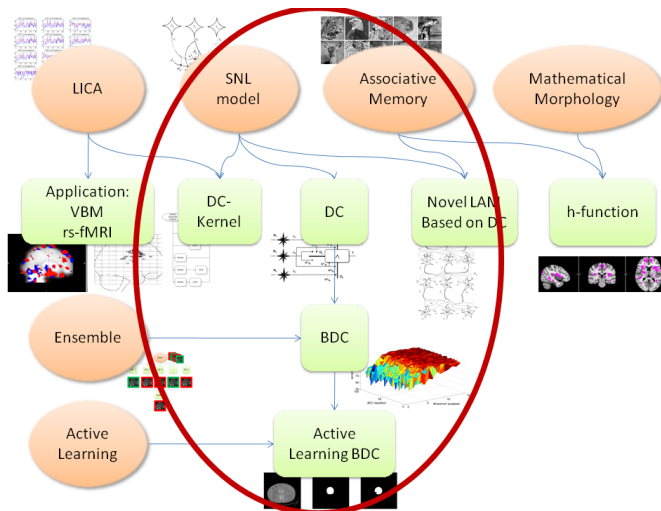
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## Dendritic computing





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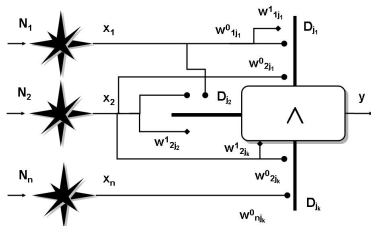
**Dendritic** Computation was introduced as a simple, fast, efficient biologically inspired method to build up classifiers for binary class problems.

**Specifically** the SLMP has been proved to perform a perfect approximation to any data distribution.

**However** SLMP suffers from over-fitting problems. Cross-validation experiments results show very poor performance.

**Proposition:** to apply a reduction factor on the size of the hyperboxes created by the SLMP learning algorithm. The results show a better balance between sensitivity and specificity, increasing the classifier accuracy.

# Illustration of the structure of a single output class SLMP



- $N_1, \dots, N_n$  - set of presynaptic neurons
- $D_j$  - the dendrites
- $(w^0_{ij}, w^1_{ij})$  - inhibitory and excitatory weights

**Algorithm 2.1** Dendritic Computing learning algorithm based on elimination.

Training set  $T = \left\{ \left( \mathbf{x}^\xi, c_\xi \right) \mid \mathbf{x}^\xi \in \mathbb{R}^n, c_\xi \in \{0, 1\}; \xi = 1, \dots, m \right\}$ ,  $C_1 = \{ \xi : c_\xi = 1 \}$ ,  $C_0 = \{ \xi : c_\xi = 0 \}$

1. Initialize  $j = 1$ ,  $I_j = \{1, \dots, n\}$ ,  $P_j = \{1, \dots, m\}$ ,  $L_{ij} = \{0, 1\}$ ,

$$w_{ij}^1 = - \bigwedge_{c_\xi=1} x_i^\xi; w_{ij}^0 = - \bigvee_{c_\xi=1} x_i^\xi, \forall i \in I$$

2. Compute response of the current dendrite  $D_j$ , with  $p_j = (-1)^{\text{sgn}(j-1)}$ :

$$\tau_j(\mathbf{x}^\xi) = p_j \bigwedge_{i \in I_j} \bigwedge_{l \in L_{ij}} (-1)^{1-l} \left( x_i^\xi + w_{ij}^l \right), \forall \xi \in P_j.$$

3. Compute the total response of the neuron:

$$\tau(\mathbf{x}^\xi) = \bigwedge_{k=1}^j \tau_k(\mathbf{x}^\xi); \xi = 1, \dots, m.$$

4. If  $\forall \xi \left( f(\tau(\mathbf{x}^\xi)) = c_\xi \right)$  the algorithm stops here with perfect classification of the training set.

5. Create a new dendrite  $j = j + 1$ ,  $I_j = I' = X = E = H = \emptyset$ ,  $D = C_1$

6. Select  $\mathbf{x}^\gamma$  such that  $c_\gamma = 0$  and  $f(\tau(\mathbf{x}^\gamma)) = 1$ .

7.  $\mu = \bigwedge_{\xi \neq \gamma} \left\{ \bigvee_{i=1}^n \left| x_i^\gamma - x_i^\xi \right| : \xi \in D \right\}$ .

8.  $I' = \left\{ i : \left| x_i^\gamma - x_i^\xi \right| = \mu, \xi \in D \right\}$ ;  $X = \left\{ \left( i, x_i^\xi \right) : \left| x_i^\gamma - x_i^\xi \right| = \mu, \xi \in D \right\}$ .

9.  $\forall \left( i, x_i^\xi \right) \in X$

- (a) if  $x_i^\gamma > x_i^\xi$  then  $w_{ij}^1 = -(x_i^\xi + \mu)$ ,  $E_{ij} = \{1\}$

- (b) if  $x_i^\gamma < x_i^\xi$  then  $w_{ij}^0 = -(x_i^\xi - \mu)$ ,  $H_{ij} = \{0\}$

10.  $I_j = I_j \cup I'$ ;  $L_{ij} = E_{ij} \cup H_{ij}$

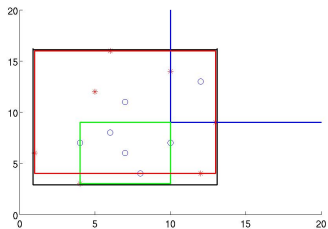
11.  $D' = \left\{ \xi \in D : \forall i \in I_j, -w_{ij}^1 < x_i^\xi < -w_{ij}^0 \right\}$ . If  $D' = \emptyset$  then goto step 2, else

$D = D' \cup C_0$ ; goto step 7

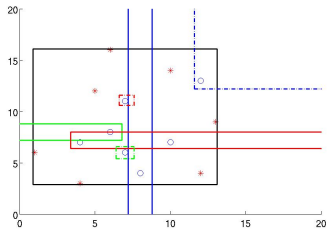
Construct a  
basic hyperbox

Adding of  
dendrites to  
remove  
misclassified  
patterns of  
class 0 that  
fall inside this  
hyperbox

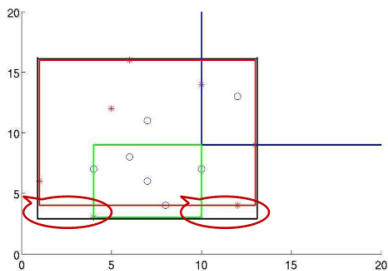
## Resulting boxes on a synthetic 2D dataset



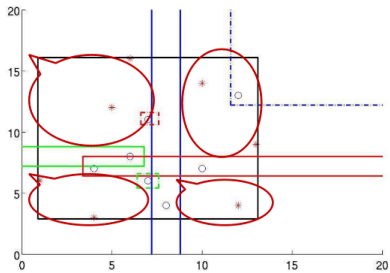
Original SLMP learning

Shrinking factor  $\alpha = 0.8$

## Resulting boxes on a synthetic 2D dataset



original SLMP learning



shrinking factor  $\alpha = 0.8$

- Better balance of specificity and sensitivity by shrinking the boundaries of the hyperbox.
- Shrink patient class regions to reduce misclassification of control samples.

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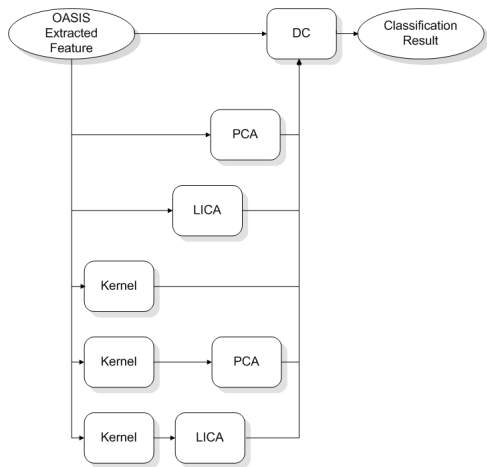
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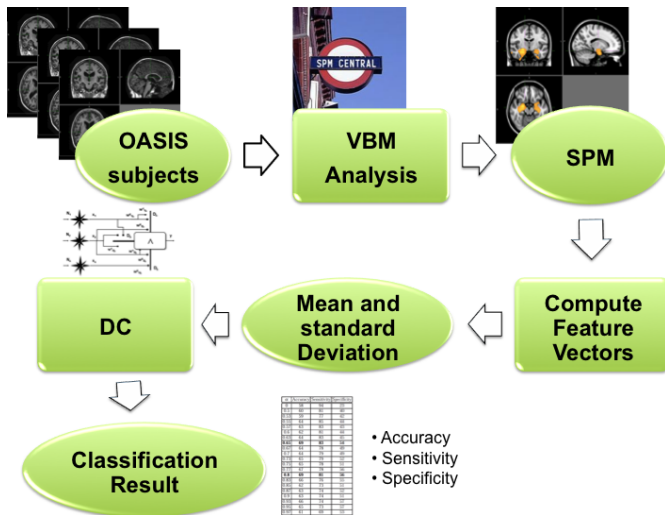
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Lattice Independent Component Analysis (LICA) and the Kernel transformation of the data as an appropriate feature extraction that improves the generalization of SLNDC







**Figure:** Pipeline of the process performed, including VBM, feature extraction and classification by DC

Method	NE	$\alpha$	$\sigma$	Accuracy	Sensitivity	Specificity
DC	-	-	-	58	94	23
DC shrinking	-	-	-	<b>69</b>	81	56
PCA - DC	1	-	-	68.25	85.5	51
LICA - DC	1	7	-	<b>72</b>	88	56
Kernel - DC	-	-	0.2512	55	98	12
Kernel - PCA - DC	8	-	0.0794	66.5	96	37
Kernel - LICA - DC	3	2	0.5012	<b>74.25</b>	96	52.5

**Table:** Summary of best results of validation experiments over AD feature database.

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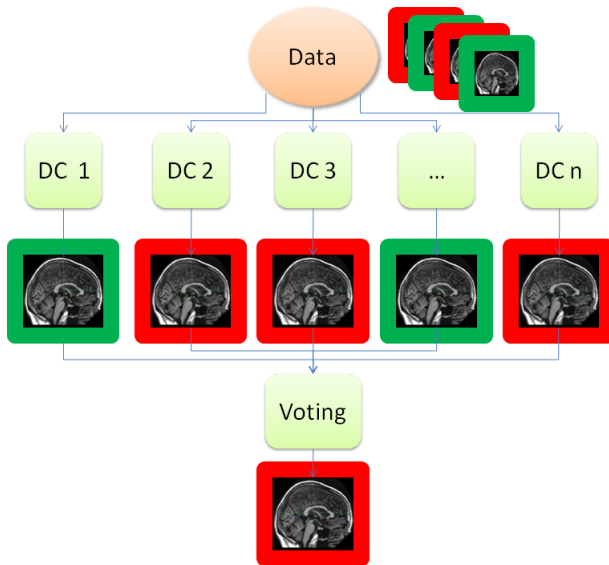
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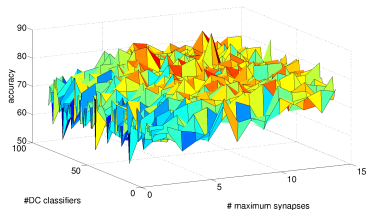
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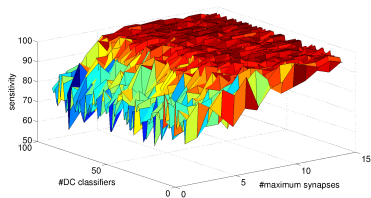
- Bootstrapped** Dendritic Classifiers (BDC) is an ensemble of weak Dendritic Classifiers, combining their output by majority voting to obtain improved classification generalization performance.
- Weak** Dendritic Classifiers are trained on bootstrapped samples of the train data setting a limit on the number of dendrites.
- There** is no additional data preprocessing.
- Results** performance and the sensitivity to the number of classifiers and the number of dendrites on the classification of Alzheimer's Disease patients, comparing with previous results obtained on the same feature database.



Average Accuracy and average Sensitivity for varying number of DC classifiers and maximum number of dendritic synapses



Accuracy



Sensitivity

Table: Best results over the OASIS data MSD features for AD detection

Classifiers	Accuracy	Sensitivity	Specificity
rbf SVM	81	89	75
LVQ1	81	90	72
LVQ2	83	92	74
rbf-DAB-SVM	85	92	78
rbfRVM-LVQ1	87	92	73
LICA - DC	72	88	56
Kernel - LICA - DC	74	96	52.5
Bootstrapped DC	<b>89</b>	<b>100</b>	<b>80</b>

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# A Novel Lattice Associative Memory Based on Dendritic Computing

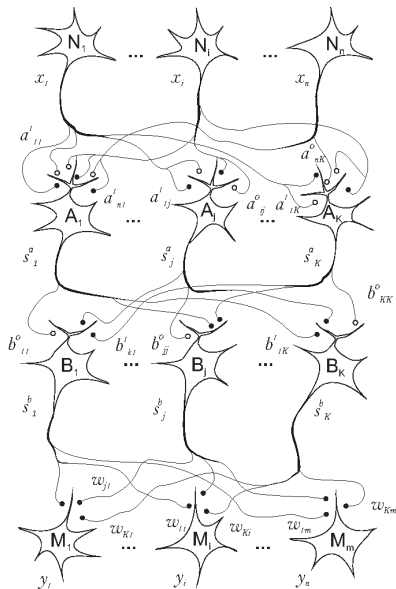
**Present** a novel hetero-associative memory based on dendritic neural computation.

**Proposed** multi-layer model

**allows** to store any finite number of input/output pattern pairs,

**complexity** grows linearly with number of stored pairs,

**extremely** robust in the presence of various types of noise and data corruption.



1.-  $N_1, \dots, N_n$  - an input layer

2.-  $A_1, \dots, A_K$  - the first hidden layer

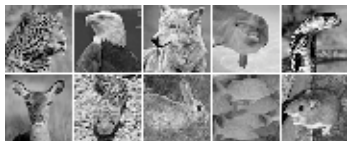
Computes the  $L_1$ -distance between the input pattern  $\mathbf{x}$  and the  $j$ th exemplar pattern  $\mathbf{x}^j$

3.-  $B_1, \dots, B_K$  - the second hidden layer

which pattern vector  $\mathbf{x}$  is closer to the exemplar pattern  $\mathbf{x}^j$ , establish the threshold  $T$ .

4.-  $M_1, \dots, M_m$  - an output layer

# Noise Robustness Experiment



**Figure:** Set of grayscale image pairs: Upper row, input images (5 Predators). Lower row corresponding output images (5 Preys).

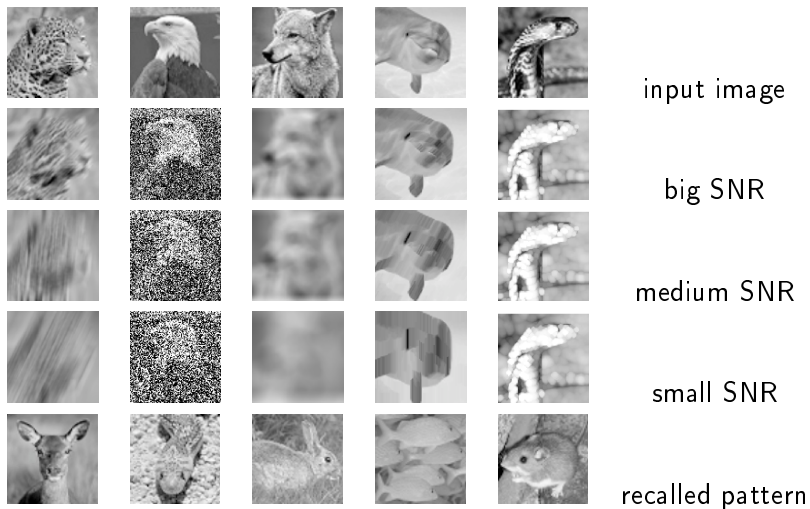


Figure: DLAM recalled patterns for diverse noise scales are identical and perfect

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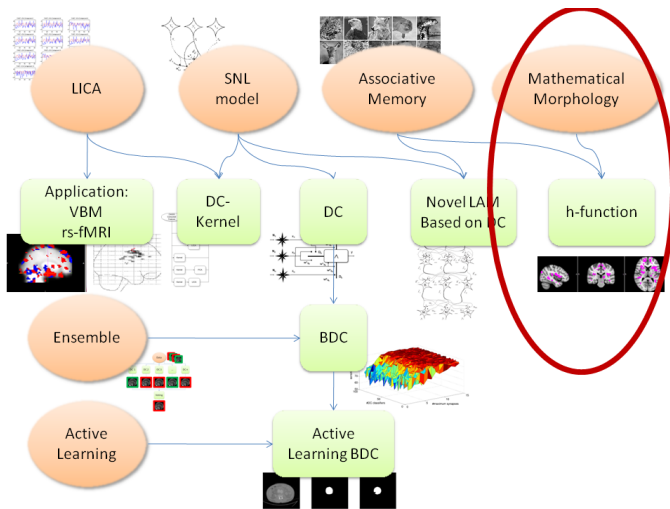
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# Multivariate Mathematical Morphology (MMM)



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# Introduction

**Approach** to define Multivariate Mathematical Morphology

**based** on the definition of a supervised ordering

**built** on the Lattice Auto-associative Memory recall  
error

**Results** on the application on resting state fMRI to discover  
functional connectivity



**General** approach consists in the application of Lattice Auto-Associative Memories (LAAMs) to the definition of a *LAAM-supervised ordering*, an specific kind of *h-ordering*.

**Allowing** the consistent definition of morphological operators on multivariate data.

**All** the required calculations are defined using the Lattice algebra operators ( $\vee$ ,  $\wedge$  and  $+$ ).

**Therefore,** LAAM-supervised ordering is faster and imposes less computational burden than the supervised orderings previously proposed.

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# Multivariate Mathematical Morphology

The two elementary morphological operators

- erosion: an operation that is distributive with the minimum

$$\varepsilon \left( \bigwedge Y \right) = \bigwedge_{y \in Y} \varepsilon(y)$$

- dilation: distributive with the maximum

$$\delta \left( \bigvee Y \right) = \bigvee_{y \in Y} \delta(y)$$

Image morphological filters:

- morphological gradient

$$g(Y) = \delta(Y) - \varepsilon(Y)$$

- the top-hat

$$t(Y) = Y - \delta(\varepsilon(Y))$$

# Multivariate ordering

**Morphological** operators are well defined for scalar images

**However** their extension to multivariate images is not straightforward

**Properties** of the morphological operators not preserve (new colors are generation)

***h*-supervised** ordering is defined

$$\mathbf{x} \leq_h \mathbf{y} \Leftrightarrow h(\mathbf{x}) \leq h(\mathbf{y}); \forall \mathbf{x}, \mathbf{y} \in X.$$

# Multivariate morphological operators

- The  $h$ -supervised erosion of a multivariate image  $\{I(p) \in \mathbb{R}^n\}_{p \in D_I}$ , with structural object  $S$ , is defined as follows:

$$\varepsilon_{h,S}(I)(p) = I(q) \text{ s.t. } I(q) = \bigwedge_h \{I(s); s \in S_p\}$$

- where  $\bigwedge_h$  is the infimum defined by the reduced ordering  $\leq_h$ , and
- $S_p$  is the structural element translated to the pixel position  $p$ .
- The  $h$ -supervised dilation  $\delta_{h,S}(I)(p)$ , has dual definition based on supremum  $\bigvee_h$ .
- $h$ -supervised morphological gradient can be defined as follows:

$$g_{h,S}(I) = h(\delta_{h,S}(I)) - h(\varepsilon_{h,S}(I)).$$

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# LAAM's $h$ -mapping

- The LAAM  $h$ -mapping is defined as the Chebyshev distance between the original pattern vector and the recall obtained from the LAAM.
- Formally, given a sample data vector  $\mathbf{x} \in \mathbb{R}^n$  and a non-empty training set  $X = \{\mathbf{x}_i\}_{i=1}^K$ ,  $\mathbf{x}_i \in \mathbb{R}^n$ , the LAAM  $h$ -mapping is given by:

$$h_X(\mathbf{c}) = d_C(\mathbf{x}^\#, \mathbf{x}),$$

- where  $\mathbf{x}_M^\# = M_{XX} \boxtimes \mathbf{x}$ ,
- function  $d_C(\mathbf{a}, \mathbf{b})$  denotes the Chebyshev distance:

$$d_C(\mathbf{a}, \mathbf{b}) = \bigvee_{i=1}^n |a_i - b_i|.$$

# Foreground LAAM $h$ -supervised ordering

- Given a training set  $X$ .
- Foreground LAAM  $h$ -supervised ordering, denoted by  $\leq_X$ , is defined on the LAAM  $h$ -mapping as follows:

$$\forall \mathbf{x}, \mathbf{y} \in \mathbb{R}^n, \mathbf{x} \leq_X \mathbf{y} \iff h_X(\mathbf{x}) \leq h_X(\mathbf{y}).$$

- The Foreground LAAM-supervised ordering generates a complete lattice  $\mathbb{L}_X$ ,
  - bottom element  $\perp_X = 0$  corresponds to the set of fixed points of  $M_{XX}$  and  $W_{XX}$ , i.e.  $h(\mathbf{x}) = \perp_X$  for  $\mathbf{x} \in \mathcal{F}(X)$
  - top element is  $\top_X = +\infty$ .



# Background/Foreground LAAM $h$ -supervised orderings

- Given disjoint background  $B$  and foreground  $F$  training sets.
- The Foreground LAAM  $h$ -mapping is independently applied to the data using  $B$  and  $F$  as training sets, obtaining mappings  $h_B$  and  $h_F$ , respectively.
- We define a Background/Foreground (B/F) LAAM  $h$ -mapping  $h_r(\mathbf{x})$  as follows:

$$h_r(\mathbf{x}) = h_F(\mathbf{x}) - h_B(\mathbf{x}),$$

which is positive for  $\mathbf{x} \in \mathcal{F}(B)$ , and negative for  $\mathbf{x} \in \mathcal{F}(F)$ .

# Background/Foreground LAAM $h$ -supervised orderings

- The Background/Foreground (B/F)  $h$ -supervised ordering, denoted  $\leq_r$ , is defined as follows:

$$\forall \mathbf{x}, \mathbf{y} \in \mathbb{R}^n, \mathbf{x} \leq_r \mathbf{y} \iff h_r(\mathbf{x}) \leq h_r(\mathbf{y}).$$

- The image of the B/F LAAM  $h$ -mapping is a complete lattice  $\mathbb{L}_r$ 
  - bottom and top elements are  $\perp = -\infty$  and  $\top = +\infty$ , respectively.

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# rs-fMRI images

- We consider rs-fMRI data of healthy controls (HC), schizophrenia patients with and without auditory hallucinations (SZA<sub>H</sub> and SZnA<sub>H</sub>, respectively).
- A seed voxel BOLD time series is used to build a LAAM, which is then applied to the remaining voxels of the brain fMRI 4D data.
- The  $h$ -function provides the functional similarity for brain network identification.
- The map obtained from the whole brain volume is thresholded to detect functional connectivity.

Two experiments performed on the rs-fMRI data:

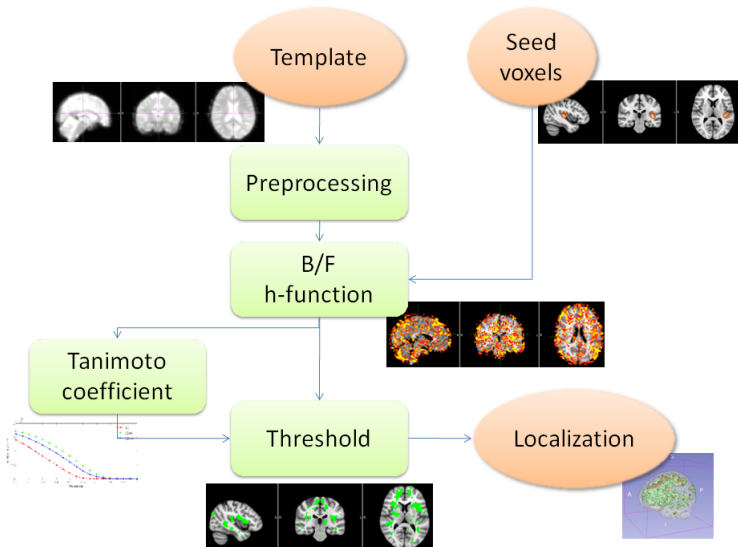
### 1 Whole brain volume group analysis

- we build one template for each population (HC, SZAH and SZnAH) by averaging the registered 4D data
- background/foreground  $h$ -function map on each template
- explore the network induced on each template by an specific localization in the left Heschl's gyrus of the brain
- optimal threshold value is decided by inspection
  - minimal Tanimoto coefficients between the functional networks of each template.
  - maximum cluster size
- visual comparison of detected networks

### 2 Classification results.

- we build the B/F  $h$ -function map related to the left Heschl's gyrus on each subject
- feature selection Pearson correlation coefficient between the  $h$ -function values and the categorical variable at each voxel site
- feature vectors are constructed as the  $h$ -function values at these sites
- results with the baseline k-NN classifiers

# Experiment 1



# Experiment 1



Figure: Foreground voxel seed site from the left Heschl's gyrus (LHG; -42,-26,10).

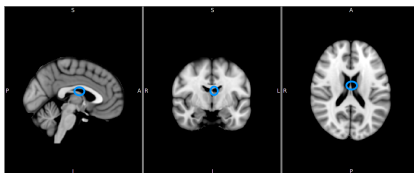
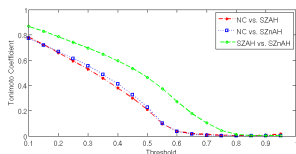
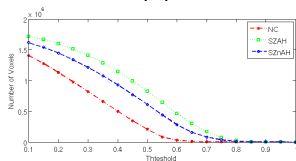


Figure: Background voxel seed site from CSF of the ventricle.



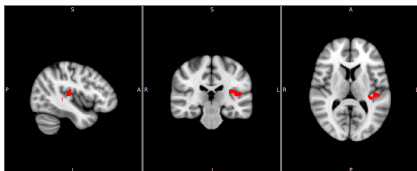
(a)



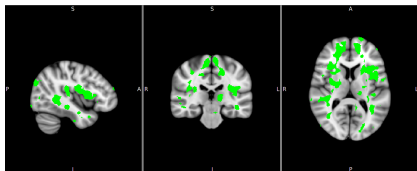
(b)

**Figure:** Effect of threshold value on the identified networks on background/foreground  $h$ -function brain map. (a) Tanimoto Coefficient comparing networks from each pair of population, and (b) size of the detected clusters.

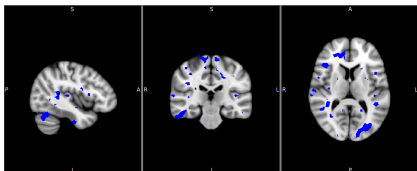




healthy controls

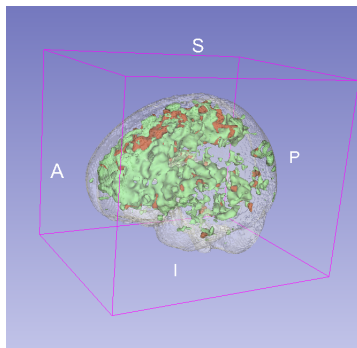


schizophrenics with  
hallucinations



schizophrenics without  
hallucinations

Figure: Networks identified by thresholding the Background/Foreground  $h$ -function induced by the pair of background/foreground seeds



**Figure:** 3D visualization of the brain networks appearing only in the SZAH population template (green), and the common networks between SZAH and SZnAH populations (brown).

# Experiment 2

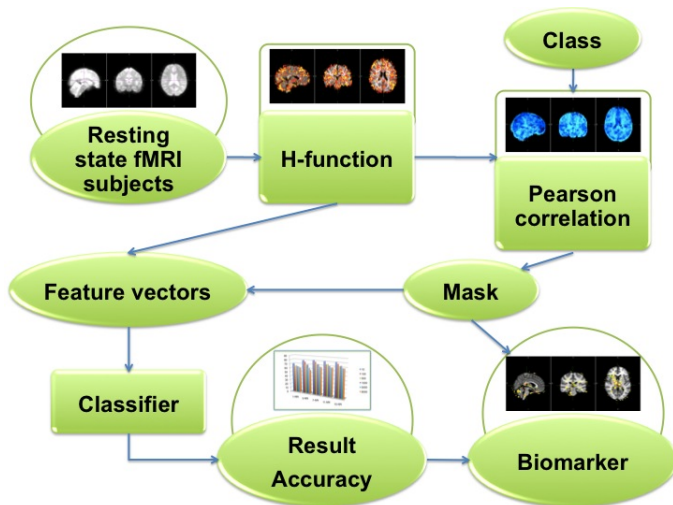
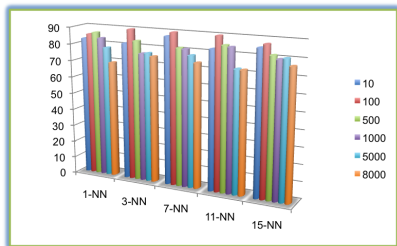
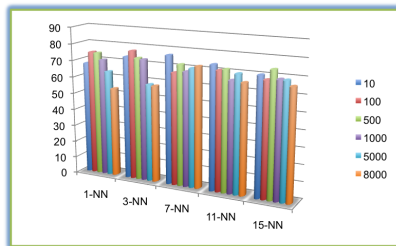


Figure: Pipeline of classification experiment



HC vs. nAH



nAH vs. AH

**Figure:** Maximum Classifier Accuracy found in 10 repetition of 10-fold cross validation for k-NN classifier  $k = 1, 3, 7, 11, 15$ . The bar colors represent different number of extracted features.

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# Conclusions: DC

**Problems:** over-fitting, degradation performance when applied cross-validation test.

**Relax** this over-fitting, found balance between sensitivity and specificity, we introduce a shrinking factor of the hyperboxes.

**Preprocessing** of the data: linear transformations (PCA), non-linear transformations (Gaussian kernel and LICA), and combinations.

**Proposed** the Bootstrapped Dendritic Classifier (BDC), which is a collection of weak SLMP trained on independently bootstrapped samples. Classification decision is made by majority voting.

**Dendritic** Lattice Associative Memory (DLAM) is a multilayer architecture of dendritic computing. DLAM possesses strong robustness against noise corruption.

# Conclusions: MMM

**Extension** of Mathematical Morphology to multivariate data, such as fMRI 4D volumes

**Definition** of reduced ordering maps by supervised classification approaches

**Lattice** Auto-Associative Memories (LAAM) recall error measured by the Chebyshev

**definition** of LAAM based Foreground and Background/Foreground reduced orderings, corresponding to one-class and two-class supervised classification approaches,

**definition** of morphological operators and filters

## Conclusions: Application

- Worked** on a set of feature vectors extracted from a subset of structural images from an Alzheimer's Disease public database (OASIS).
- Multilayer** DLAM was tested on a collection of grayscale images subjected to diverse degrees of noise corruption.
- Applying** LAAM to resting state fMRI data of Schizophrenia patients versus controls we obtain discriminant brain networks that can be appreciated visually and also serve for feature extraction purposes with good classification performance results using baseline k-NN classifiers.



Contributions of Lattice Computing to Medical Image Processing  
Thesis dissertation

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Advisor: Prof. Dr. Manuel Graña

*Thank you very much for your attention!*